# An Ultra Low-Power Low-Noise Neural Signal Acquisition Amplifier for ECoG Applications

# Jin-Young Son<sup>1</sup> and Hyouk-Kyu Cha<sup>a</sup>

Department of Electrical and Information Engineering, Seoul National University of Science and Technology E-mail : <sup>1</sup>jyson@seoultech.ac.kr

Abstract – An ultra low-power, low-noise neural recording amplifier for electrocorticography (ECoG) applications is presented. The proposed AC-coupled capacitive-feedback neural amplifier employing a gain-boosted inverter-stacked operational transconductance amplifier with floating-body technique achieves an enhanced input noise performance despite consuming limited power. The designed amplifier IC achieves a closed-loop gain of 40 dB, integrated input-referred noise of 6.3  $\mu$ Vrms within 520 Hz bandwidth while dissipating 15.5 nW of power at 1-V supply voltage. The IC is implemented using 65-nm CMOS process and occupies 0.051 mm<sup>2</sup> of die area. *Keywords*—neural recording amplifier, floating-body, gainboosting, inverter-stacked OTA, ECoG

#### I. INTRODUCTION

Multi-channel neural signal recording systems in brainmachine-interfaces can be used to diagnose and analyze various neurological disorders, with the ultimate goal of improving the understanding of the brain and its highly complex functions [1]-[9].

The recorded neural signals of interest include action (AP)/spike, local field potential (LFP), potential electroencephalogram (EEG), and electrocorticography (ECoG). Among these signals and acquisition methods, ECoG has emerged as an attractive approach and solution to neurological activity recording because it offers better resolution than EEG, and is less invasive than AP/LFP recording [9]. The ECoG signal is the electrical activity of cerebral cortex recorded by attaching flat electrodes directly on the exposed brain surface. It is the sum of the electrical activity of a large number of neurons of about 100-10000 observed and has an amplitude of several hundred  $\mu V$  to several mV in the 1-300 Hz frequency band. Thus, the ECoG signal recording front-end IC requires less operation power in comparison to spike recording due to its narrow signal bandwidth and can acquire neural signals without motion artifacts caused by the patient's movement.

One of the most important blocks in a neural recording system is the neural signal acquisition amplifier, which is usually the first analog signal processing block after the multi-electrode array (MEA). In order to incorporate multichannel operation, ultra-low-power operation is required in the individual building block to avoid potential damage to the nerve tissue from heat flux due to the excessive power dissipation of the IC. In addition, to accurately record weak neural signals with sufficient signal to noise ratio, a high gain amplification with low input-referred noise performance is critical in the design of the front-end amplifier.

While AC-coupled, capacitive-feedback topologies are widely used as neural amplifiers to block large DC offsets at electrode-tissue interfaces, the core operational transconductance amplifier (OTA) in this closed-loop circuit mostly decides the overall performance of the neural signal amplifier and thus the power-noise tradeoff needs to be carefully addressed in the design process. To achieve good noise performance at low power consumption, many OTA circuit topologies have been presented previously. Topologies such as current-mirror-based OTA [1], foldedcascode [2], [3], complementary current-reuse [4], [5], and inverter-stacking [6] have been proposed in designing the first stage OTA. Current-mirror-based OTA has the advantage of achieving a large output swing with relatively simple design process, but is known to be less power efficient. Folded-cascode architecture is a well-established circuit topology which has a large input-range, but its power efficiency is not as good as the current-reuse OTA. The current-reuse OTA with PMOS and NMOS input pair offer a good balanced performance in key performance parameters but inverter-stacked architecture achieves superior powernoise tradeoff performance, while sacrificing output voltage swing due to the stacks.

In this paper, an AC-coupled, capacitive-feedback neural recording amplifier which employs a power-efficient OTA with improved noise performance is presented for ECoG applications. The OTA is based on a gain-boosted inverterstacked architecture with floating-body input transistors for enhanced transconductance and power efficiency. Although chopper stabilization is a widely-used technique to upmodulate the low-frequency flicker noise, it greatly increases the complexity of the overall circuit and thus is not employed in this design. Section II discusses the circuit design details of the proposed amplifier. Section III presents the experimental results and the conclusions are given in Section IV.

a. Corresponding author; hkcha@seoultech.ac.kr

Manuscript Received Aug. 11, 2023, Revised Aug. 31, 2023, Accepted Sep. 1, 2023

This is an Open Access article distributed under the terms of the Creative Commons Attribution Non-Commercial License (<u>http://creativecommons.org/licenses/by-nc/4.0</u>) which permits unrestricted non-commercial use, distribution, and reproduction in any medium, provided the original work is properly cited.



Fig. 1. The block diagram of a general neural recording system-on-chip.



Fig. 2. The circuit schematic of proposed LNA.

### II. CIRCUIT DESIGN

The block diagram of a general neural recording IC architecture for recording and processing of neural signals is shown in Fig. 1. The IC is comprised of a neural amplifier as the first stage which is the dominant block that decides the overall noise performance of the recording system. The neural amplifier block usually provides a large fixed gain to boost the weak neural signal at the MEA interface. A programmable gain amplifier (PGA) with tunable gain and filtering functions follows the neural amplifier which enables the AFE to process neural signals with various amplitudes. An analog multiplexer (MUX) block follows the PGA to reduce the number of dedicated analog-to-digital converters (ADC) for power and area reduction. Finally, the ADC is used to digitize the recorded signal for further digital processing and wireless transmission to an external device. This work only includes the single-channel neural recording amplifier.

Fig. 2 shows the closed-loop schematic of the proposed low-noise neural amplifier. As the core OTA has total three



ᄩ M -11 Floating-body

Ma

м

V<sub>⊵,N</sub>⊣[

止

M<sub>c2</sub>

Fig. 3. The core circuit schematic of proposed OTA.

TABLE I. TRANSISTON SIZE OF THE OTA.	TABLE I.	Transistor	size	of the C	DTA.
--------------------------------------	----------	------------	------	----------	------

Transistor	Width/Length (µm/µm)		
M1	60/3.5		
M2	20/10		
M3	50/4		
M4	22.5/9		
Mgb1	2.4/1		
Mgb2	0.58/5		
Mgb3	2.6/1		
Mgb4	0.58/5		
Mc1	10/3		
Mc2	2/5		

pairs of input nodes (M<sub>1</sub>+M<sub>4</sub>, M<sub>2</sub>, M<sub>3</sub> in Fig.3), three pairs of split capacitive feedback loops are used. The closed-loop voltage gain of neural amplifier is set to be at 40 dB, which is determined by the ratio of the total input capacitor Cin and the feedback capacitor Cf. The input referred noise of the neural amplifier with capacitive feedback is expressed as;

$$\overline{v_{n,cl}^2} = \left(\frac{C_{in} + C_f + C_p}{C_{in}}\right) \cdot \overline{v_{n,ol}^2} \tag{1}$$

where  $C_P$  is the gate parasitic capacitance of the input transistor and  $v_{n,ol}^2$  is the input referred noise of the core OTA. Since the capacitors C<sub>in1</sub> and C<sub>f1</sub> are connected to two pairs of input transistors M1 and M4, the contribution of the parasitic capacitance of the input transistor in the feedback loop is twice of other feedback loops. Therefore, considering the noise contribution from the input transistor parasitic capacitance, the size of capacitors  $C_{\text{in1}}$  and  $C_{\text{fl}}$  is set to be twice the value of other capacitors. The values of each capacitors used for the closed-loop feedback are also shown in Fig. 2.



Fig. 4. The circuit schematic of replica-based bias circuit for the core OTA.

Fig. 3 shows the schematic of proposed core OTA circuit. To maximize the transconductance of the input pairs under limited power, the transistors are sized with large W/L ratios and biased in subthreshold. The OTA is designed based on the inverter-stacking scheme proposed in [6]. In this scheme, four pairs of input transistors are stacked and the bias current is four times reused, thus greatly improving the power efficiency of the circuit. The input transconductance is thus boosted by four times with the same current consumption, and can achieve low noise floor and wide bandwidth. The total transconductance Gm of the inverter-stacked OTA is expressed as the following equation;

$$G_m = (g_{m1} + g_{m2} + g_{m3} + g_{m4}) \approx 4g_{m,in} \qquad (2)$$

where  $g_{mi}$  is transconductance of input transistor  $M_i$ . To further increase the Gm of OTA, the body terminal of all input transistors are AC-coupled to the gate terminal through the capacitor and are DC-floated [8]. Because the body terminal is AC-coupled to the gate terminal, the small-signal voltage of body terminal can swing along the gate voltage through the body to gate capacitance. Thus, by using the floating body technique, the equivalent  $G_m$  of OTA increases as;

$$G_m \approx 4g_{m,in} + 4g_{mb,in} \tag{3}$$

where  $g_{mb,in}$  is the body transconductance of input transistor. By using the  $g_{mb}$  of input transistor, the equivalent  $G_m$  of OTA increases, and the resulting simulated bandwidth is improved by 35% while the input referred noise performances is improved by over 10% at equal power consumption. For the AC-coupling capacitors between the gate and the body terminal, metal-oxide-metal (MOM) capacitor is used. The size of added MOM capacitor is determined by trade-off between active area and OTA performances. In this design, a 250 fF capacitor is used for each input transistor.

In order to obtain a sufficiently large open-loop gain using deep sub-micron process, gain boosting technique is applied to the inverter-stacked architecture. At the gain boosting stage, a common source stage with an active current source load was used for simple circuit configuration. The sizes of the transistors used in the OTA core is presented in Table I.



Fig. 5. The chip micrograph of proposed neural amplifier.

The overall input-referred noise of the proposed OTA is expressed as;

$$\overline{v_n^2} = \overline{v_{n,th}^2} + \overline{v_{n,l/f}^2} = \frac{8kT\gamma}{G_m} + \left(\frac{K_f}{C_{ox}4WL} \cdot \frac{l}{f}\right)$$
(4)

where  $\overline{v_{n,th}^2}$  and  $\overline{v_{n,lf}^2}$  are the thermal noise and 1/f noise, respectively. T is temperature, k is Boltzmann's constant, K<sub>f</sub> is a process-dependent parameter, and  $\gamma$  is excess noise constant. By using the floating-body technique, the equivalent G<sub>m</sub> of OTA is increased, and the thermal noise of OTA is reduced. Since the noise contribution from the input transistors dominates the entire noise floor, the noise contribution of cascode and gain boosting devices is ignored.

For the gate bias of the input core transistors in the middle part of the stack  $(M_2, M_3)$ , a replica-based bias branch shown in Fig. 4, is used to generate accurate voltages to ensure robust operation despite process, voltage, temperature (PVT) variation. For the common-mode feedback (CMFB) circuit, a resistor-averaged topology is utilized to stabilize the common-mode voltages.

# III. RESULTS AND DISCUSSIONS

The proposed neural amplifier is designed and fabricated using 65-nm CMOS process. An on-chip unity-gain buffer is included for testing. The IC is assembled using chip-onboard packaging and measured on a FR4 printed-circuitboard. Fig. 5 shows the micrograph of the fabricated chip and the active area is 0.051 mm<sup>2</sup>.

Fig. 6 shows the measured frequency response of the neural amplifier. The amplifier has 40 dB of mid-band voltage gain, with 0.3 Hz of high-pass cutoff frequency and 520 Hz of low-pass cutoff frequency. The -3 dB bandwidth of LNA is sufficient to cover the bandwidth of the ECoG signal.

Fig. 7 shows the input-referred noise spectrum. The integrated input-referred noise within the -3 dB bandwidth is about 6.3  $\mu$ Vrms, and the input-referred noise within the 1 Hz to 300 Hz ECoG signal band is 5.1  $\mu$ Vrms.



Fig. 6. Measured closed-loop gain response.



Fig. 7. Measured input-referred noise response.

Parameter	This work	[11]	[12]	[13]
Supply (V)	1	2.5	1	0.6
Gain (dB)	40	-	40	36.9
BW (Hz)	520	1k	150	250
Input referred noise (µVrms)	6.3	2.78	112 nV/ sqrt(Hz)	6.52
Power (nW)	15.5*	2.98µ	1.08µ	28
Noise efficiency factor	1.33**	2.35	-	2.64
Power efficiency factor	1.77**	13.8	-	4.18
CMRR (dB)	>80*	76	82	55
PSRR (dB)	>80*	82	68	67
Area (mm <sup>2</sup> )	0.051	0.0023	0.085	-
Process (nm)	65	65	65	65
Application	ECoG	ECoG	ECoG	ECG

TARIFII	Performance	summary	of the	designed	neural	amplifier
IADLE II	. Feriormance	summary	or the	uesigneu	neurai	ampimer.

\*Simulated value, \*\*Calculated with simulated power consumption

Table II shows the measured performance summary and compares with other neural recording amplifiers operating at low frequency bands, implemented using similar process technologies. The noise efficiency factor (NEF) and power efficiency factor (PEF) [1] parameters are used to compare the neural signal recording amplifier noise-power trade-off performance. The total current consumption of the proposed LNA is 15.5 nA, achieving 1.33 and 1.77 of NEF and PEF, respectively. In comparison to similar works, the proposed neural amplifier achieves enhanced noise-to-power trade-off performances.

# IV. CONCLUSION

The ultra low-power gain-boosted inverter-stacked OTA with floating-body is proposed for improved input-referred noise performance. The designed closed-loop neural signal acquisition amplifier employing the proposed OTA achieves 40 dB of voltage gain, 6.3  $\mu$ Vrms of input referred noise, and 520 Hz of -3 dB bandwidth while consuming 15.5 nW of power consumption at 1-V supply. The amplifier is implemented using 65 nm CMOS process and occupies 0.051 mm<sup>2</sup> of die area.

## ACKNOWLEDGEMENT

This research was funded by Basic Science Research Program through the National Research Foundation of Korea (NRF) funded by the Ministry of Science and ICT (MSIT), (NRF-2018R1C1B6003088). The chip fabrication and EDA tool were supported by the IC Design Education Center (IDEC).

### REFERENCES

- R. R. Harrison and C. Charles, "A low-power low-noise CMOS amplifier for neural recording applications", *IEEE J. Solid State Circuits*, vol. 38, no. 1, pp. 958-965, Jun. 2003
- [2] W. Wattanapanitch et al., "An energy-efficient micropower neural recording amplifier", *IEEE Trans. Biomedical Circuits and Sys.*, vol. 1, no. 2, pp. 136–147, Jun. 2007.
- [3] D. Choi et al., "A low-power neural signal acquisition analog front-end IC for closed-loop neural interfaces", *IEIE J. of Semicond. Tech. and Science*, vol.22, no.5, pp.368-375, Oct. 2022
- [4] L. Liu et al., "800 nW 43 nV/√Hz neural recording amplifier with enhanced noise efficiency factor", *IET Electronics Lett.*, vol. 48, no. 9, pp. 479-480, Apr. 2012
- [5] H. S. Kim et al., "An ultra low-power low-noise neural recording analog front-end IC for implantable devices", *IEIE J. of Semicond. Tech. and Science*, vol.18, no.4, pp.454-460, Aug. 2018
- [6] L. Shen et al., "A 1-V 0.25-μW inverter stacking amplifier with 1.07 noise efficiency factor," *IEEE J. Solid-State Circuits*, vol. 53, no. 3, pp. 896-905, Jan. 2018

- [7] H. Chandrakumar and D. Markovic. "An 80-mVpp linear-input range, 1.6-GΩ Input ompedance, lowpower chopper amplifier for closed-loop neural recording that is tolerant to 650-mVpp common-mode interference", *IEEE J. of Solid-State Circuits*, vol. 52, no. 11, pp. 2811-2827, Nov. 2017
- [8] S.-I. Chang et al., "BioBolt: A minimally-invasive neural interface for wireless epidural recording by intraskin communication," 2011 Symp. VLSI Circuits, pp. 146-147, Jun. 2011
- [9] S. Ha et al., "Silicon-integrated high-density electrocortical interfaces", Proc. of the IEEE, vol.105, pp. 11-33, Jan. 2017
- [10] M. S. J. Steyaert et al., "A micropower low-noise monolithic instrumentation amplifier for medical purposes," *IEEE J. Solid-State Circuits*, vol. SC-22, pp. 1163–1168, Dec. 1987.
- [11] W. A. Smith et al., "A scalable, highly-multiplexed delta-encoded digital feedback ECoG recording amplifier with common and differential-mode artifact suppression," 2017 Symp. VLSI Circuits, pp. 172-173, Jun. 2017
- [12] W. A. Smith et al., "Exploiting electrocorticographic spectral characteristics for optimized signal chain design: A 1.08  $\mu$ W analog front end with reduced ADC resolution requirements," *IEEE Trans. Biomedical Circuits and Sys.*, vol. 10, no. 6, pp. 1171–1180, Dec. 2016.
- [13] Y.-P. Chen et al., "An injectable 64 nW ECG mixedsignal SoC in 65 nm for arrhythmia monitoring," *IEEE J. Solid-State Circuits*, vol. 50, no. 1, pp. 375-390, Jan. 2015
- [14] T. Yanagisawa et al., "Electrocorticographic control of a prosthetic arm in paralyzed patients", *Ann. Neurol.*, vol. 71, no. 3, pp. 353-361, Mar. 2012



**Jin-Young Son** received the B.S and M.S. degrees in electrical and information engineering from Seoul National University of Science and Technology, Seoul, Korea, in 2019 and 2021, respectively. Since 2021, he has been with Qualitas Semiconductor, Seoul, Korea, as an analog IC design engineer. His research interest includes

the design of ultra low-power sensor interface analog frontend and ADC IC for biomedical applications.



**Hyouk-Kyu Cha** received the B.S. and Ph.D. degrees in electrical engineering at Korea Advanced Institute of Science and Technology (KAIST), Daejeon, Korea, in 2003 and 2009, respectively.

From 2009 to 2012, he was a Scientist with the Institute of Microelectronics, (IME), Agency for

Science, Technology, and Research (A\*STAR), Singapore, where he was involved in the research and development of analog/RF ICs for biomedical applications.

Since 2012, he has been with the Department of Electrical and Information Engineering, Seoul National University of Science and Technology, Seoul, Korea, where he is now a Professor. His research interests include low-power CMOS analog/RF IC and system design for biomedical devices.